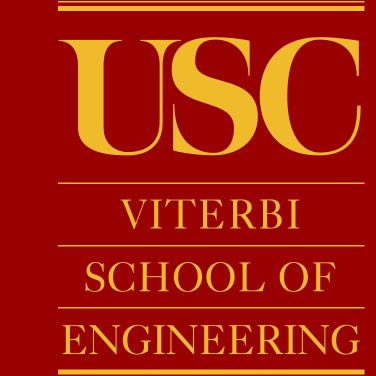


Control of muscle strain energy as a robust means to produce slow and accurate finger movements: Proof of concept via hardware and cadaver implementation



Heiko Hoffmann, Jason Kutch, Manish Kurse, and Francisco Valero-Cuevas

Biomedical Engineering and Biokinesiology and Physical Therapy, University of Southern California

Motivation

The neural control of finger movements is unknown.

Existing motor control hypotheses have not been tested on realistic systems approximating the structure of the anatomical hand.

To test these hypotheses, we created a computer-controlled system to drive a mechanical finger and human cadaveric fingers [1].

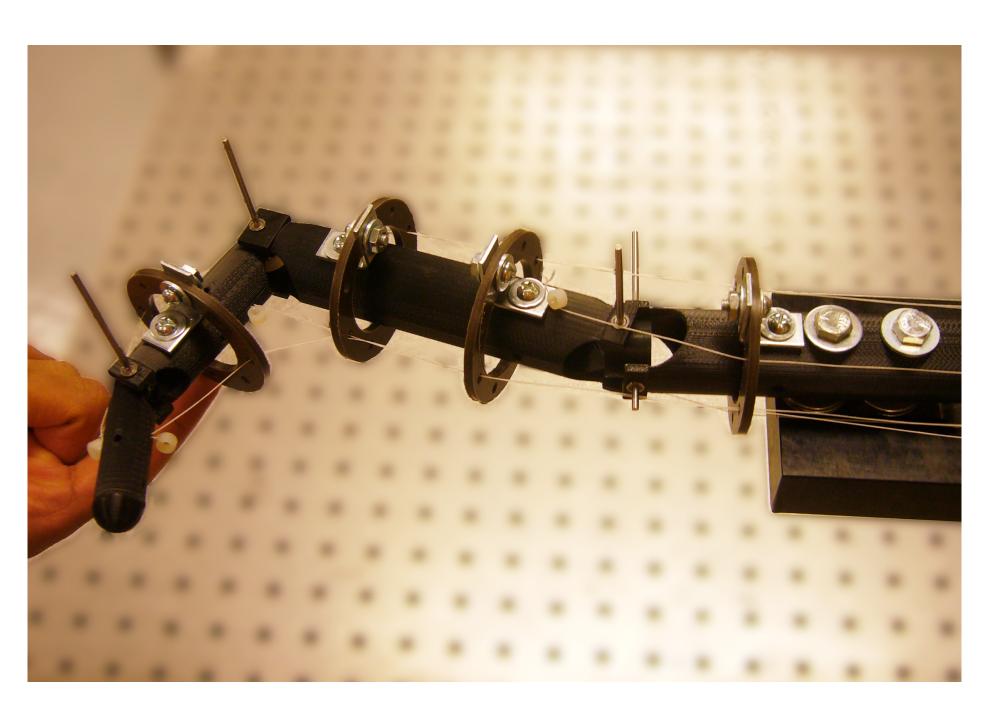
We tested two commonly-proposed motor control strategies:

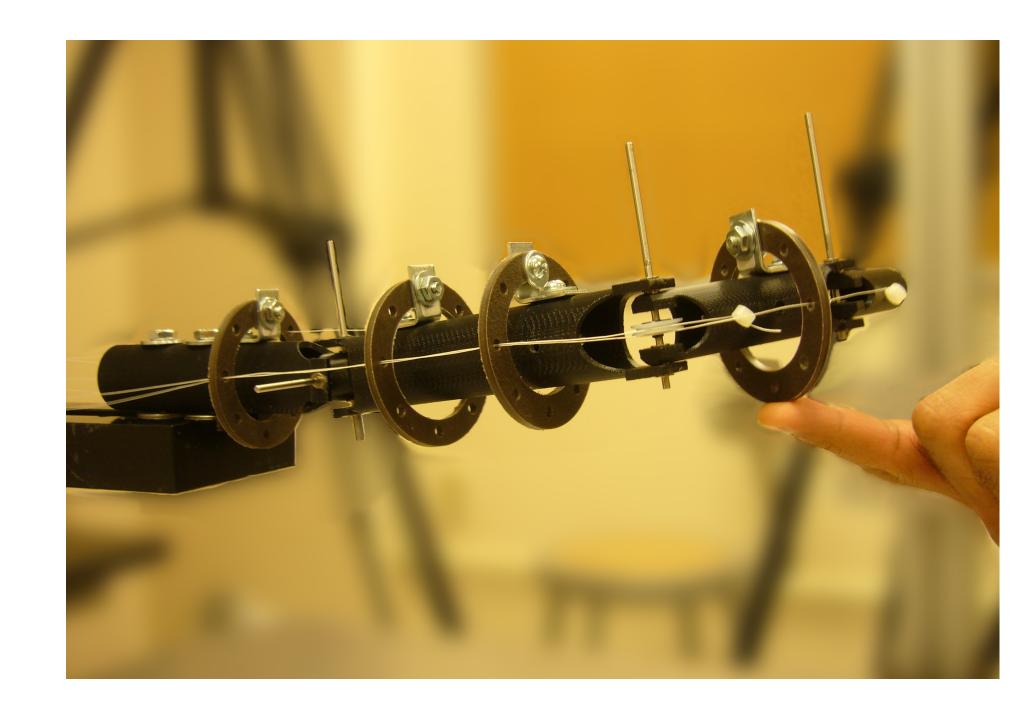
Force control: a low-level controller applies a given force pattern to the tendons, Strain-energy control: a controller sets the rest lengths of muscles, here, simulated as Hookean springs.

[1] Valero-Cuevas FJ, Towles JD, and Hentz VR. J Biomech 33: 1601-1609, 2000.

Setup

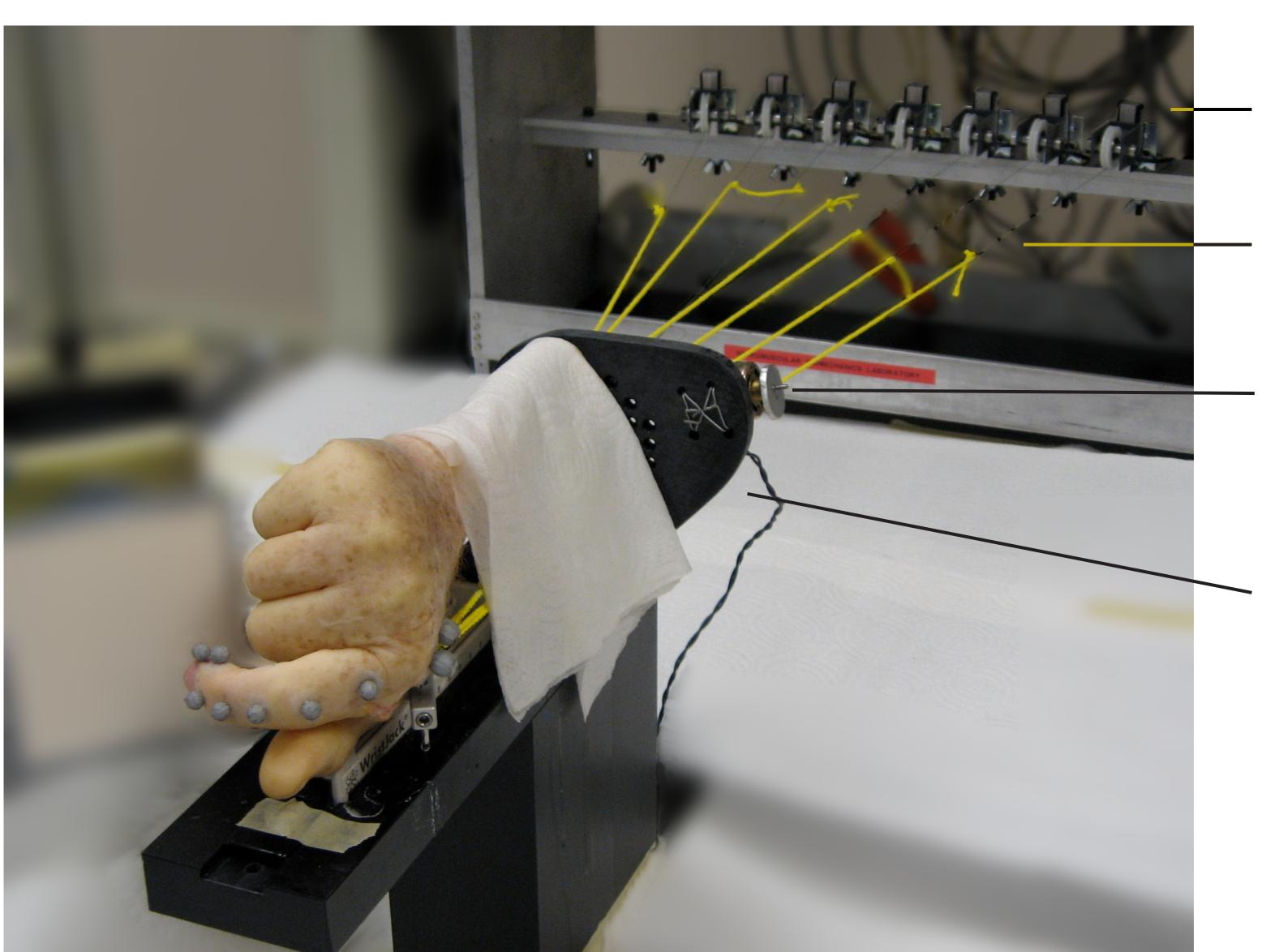
The computer-controlled system drives seven motors, each connected to a spindle. Strings winding on the spindles pull either on a mechanical finger or on all seven tendons of a human cadaveric index finger. Real-time feedback is measured for each tendon's force and excursion.





The four-degrees-of-freedom mechanical finger is equipped with polyoxymethylene disks that allow alternative tendon-routing paths. We mimicked the main routing paths in the index finger.

The cadaver hand is mounted on a wrist jack, which fixed the metacarpal and radius bones.



Load cells

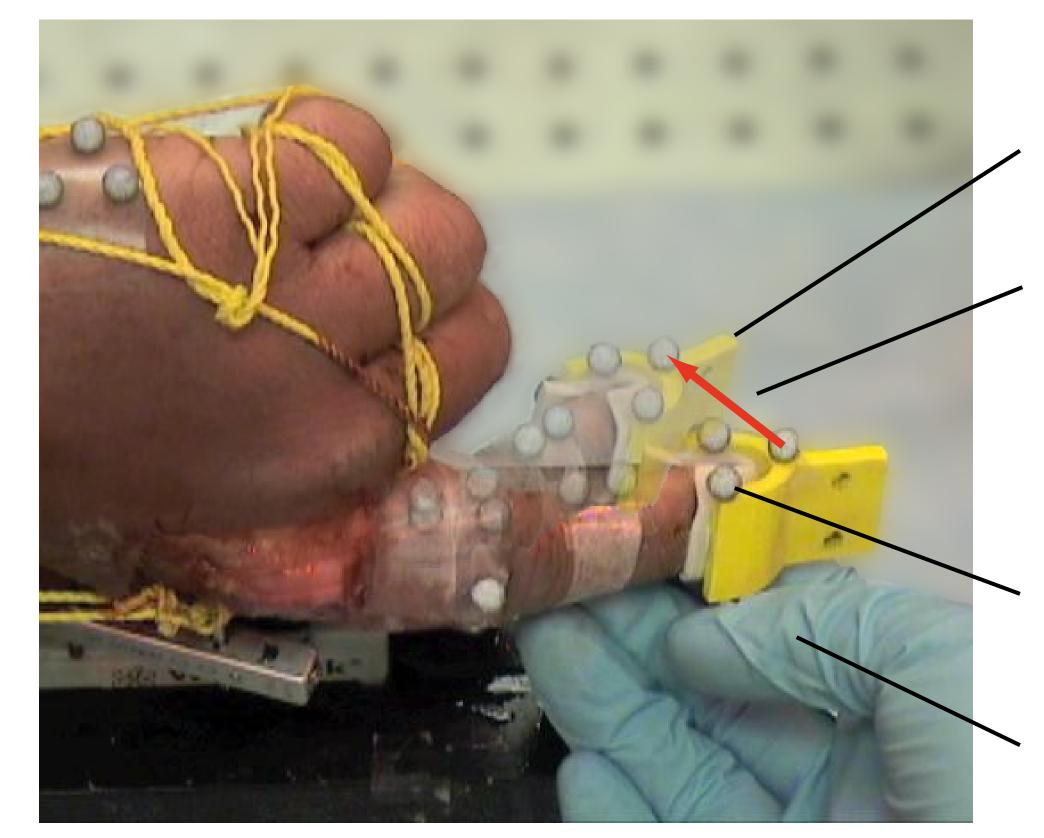
Fishing cords

Vibration device to reduce stiction

Nylon cords are routed through Polyoxymethylene plastic (Delrin)

Perturbation Experiment and Results

Under force or strain-energy control, the cadaveric index finger was manually perturbed and the resulting reaction observed.



Equilibrium posture

Relaxation:

A finger-tip motion is normalized by projecting the tip's position onto the line (red arrow) between start and equilibrium point.

Vicon motion-tracking markers

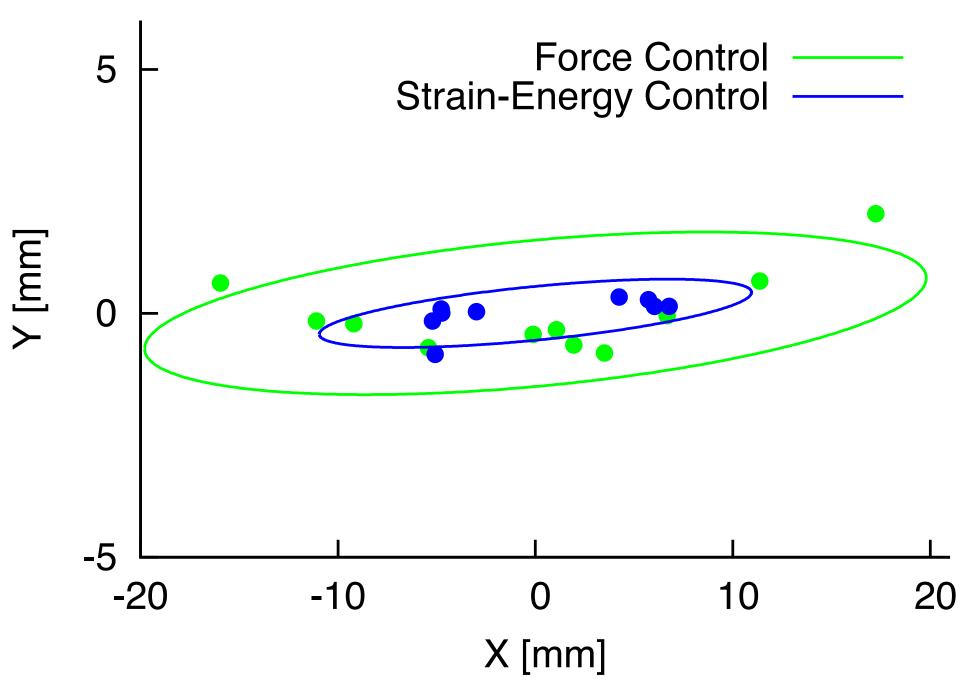
Manual perturbation

Force Control: Pulling force on both extensor tendons: 8 N, on the other five tendons: 2 N Strain-Energy Control: Spring stiffness on all seven tendons: 3 N/mm, Initial strain: 1 mm

Perturbation Reaction

Passive Mechanics Force Control Strain-Energy Control 0.5 1 2 Time [s]

Distribution of Convergence Points



Relaxation Times

Force Control: $0.69 \pm 0.13 \text{ s}$ (mean $\pm \text{SD}$, n = 4) Strain-Energy Control: $0.063 \pm 0.017 \text{ s}$ (n = 5) Dots are points of convergence of the finger tip after single perturbations. Ellipses show boundary of 95% variance.

Conclusions

We have a new paradigm to compare and contrast alternative neural controllers, while fully considering the anatomical complexity of the hand.

Strain-energy control was more robust than force control, reacting faster to perturbations and having lower hysteresis. In the mechanical finger, we could not stabilize desired postures using constant force patterns.

The hand biomechanics limit the number of feasible control strategies. A strategy that relies on a constant force pattern to result in a desired equilibrium point is infeasible.

Acknowledgments: This work was funded in part by grants NIH R01 050520 and NIH R01 052345 to FVC. We thank Drs VR Hentz, C LeClercq, and I Fassolla for their expert surgical assistance.